



INVESTOR IN PEOPLE

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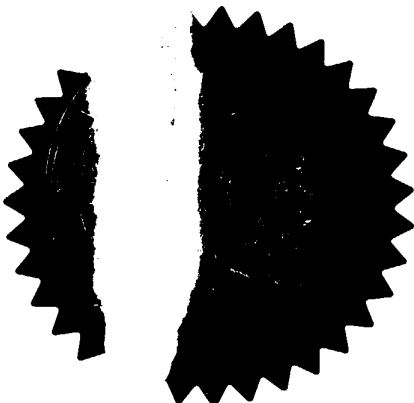
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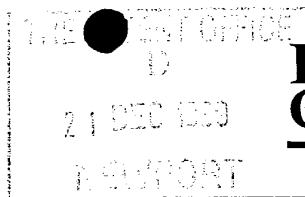
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21 DEC 1999

21DEC99 E500552-1 002865
P01/7790 0.00-9930000.6 NP10 800

1. Your reference	PHAG / P21511GB		
2. Patent application number (The Patent Office will fill in this part)	9930000.6		
3. Full name, address and postcode of the or of each applicant (underline all surnames)	Phaeton Research Ltd 2 Faraday Building Highfields Science Park University Boulevard Nottingham NG7 2QP United Kingdom United Kingdom		
Patents ADP number (if you know it)	7803521001.03		
If the applicant is a corporate body, give the country/state of its incorporation	United Kingdom		
4. Title of the invention	AN INGESTIBLE DEVICE		
5. Name of your agent (if you have one)	ERIC POTTER CLARKSON		
"Address for service" in the United Kingdom to which all correspondence should be sent (including the postcode)	PARK VIEW HOUSE 58 THE ROPEWALK NOTTINGHAM NG1 5DD		
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Description 33

Claims(s) 12

Abstract 1

Drawing(s) 12 *12*

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Priority Documents 0

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Statement of inventorship and right to grant of a patent (*Patents Form 7/77*) NO

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AN INGESTIBLE DEVICE

This invention relates to an ingestible device. In particular the invention relates to such a device in the form of a capsule that is intended to release
5 a controlled quantity of a substance, such as a pharmaceutically active compound, foodstuff, dye, radiolabelled marker, vaccine, physiological marker or diagnostic agent at a chosen location in the gastrointestinal (GI) tract of a mammal. Such a capsule is sometimes referred to as a "Site-Specific Delivery Capsule", or SSDC.

10

SSDC's have numerous uses. One use of particular interest to the pharmaceutical industry involves assessing the absorption rate and/or efficacy of a compound under investigation, at various locations in the GI tract. Pharmaceutical companies can use data obtained from such
15 investigations, eg. to improve commercially produced products.

Several designs of SSDC are known. One design of capsule intended for use in the GI tract of a mammal is disclosed in "Autonomous Telemetric Capsule to Explore the Small Bowel", Lambert *et al*, Medical &
20 Biological Engineering and Computing, March 1991. The capsule shown therein exhibits several features usually found in such devices, namely:

- a reservoir for a substance to be discharged into the GI tract;
- 25 - an on-board energy source;
- a mechanism, operable under power from the energy source, for initiating discharge of the substance from the reservoir;
- 30 - a switch, operable remotely from outside the body of the mammal,

for initiating the discharge; and

- a telemetry device for transmitting data indicative of the status, location and/or orientation of the capsule.

5

Also, of course, the dimensions of the capsule are such as to permit its ingestion via the oesophagus; and the external components of the capsule are such as to be biocompatible for the residence time of the capsule within the body.

10

The capsule disclosed by Lambert *et al* suffers several disadvantages. Principal amongst these is the complexity of the device. This means that the capsule is expensive to manufacture. Also the complexity means that the capsule is prone to malfunction.

15

For example, the capsule disclosed by Lambert *et al* includes a telemetry device that is initially retracted within a smooth outer housing, to permit swallowing of the capsule via the oesophagus. Once the capsule reaches the stomach, gastric juice destroys a gelatin seal retaining the telemetry device within the housing. The telemetry device then extends from the housing and presents a rotatable star wheel that engages the wall of the GI tract. Rotations of the star wheel generate signals that are transmitted externally of the capsule by means of an on-board RF transmitter powered by a battery within the capsule housing.

20

This arrangement may become unreliable when used in mammals whose GI motility is poor or whose gastric juice composition is abnormal.

There is a risk of malfunction of the rotating part of the telemetry device, and the method of operation of the capsule is generally complex.

30

The space needed to house the telemetry device within the capsule during swallowing/ingestion is unusable for any other purpose when the telemetry device is extended. Therefore the Lambert *et al* capsule is not
5 space-efficient. This is a serious drawback when considering the requirement for the capsule to be as small as possible to aid ingestion.

Also the Lambert *et al* disclosure details the use of a high frequency (>100 MHz) radio transmitter for remotely triggering the release of the
10 substance from the capsule into the GI tract. The use of such high frequencies is associated with disadvantages, as follows:

When power is transmitted to the capsule whilst it is inside the GI tract the energy must pass through the tissue of the mammal that
15 has swallowed the capsule. The transmission of this power through the body of the mammal may result in possible interactions with the tissue which at some power levels may lead to potential damage to that tissue.

20 The higher the frequency of energy transmission the higher the coupled power for a given field strength. However, as the frequency is increased the absorption of the energy by the body tissue also increases. The guidelines for the exposure of humans to static and time varying electromagnetic fields and radiation for the
25 UK are given in the National Radiological Protection Board (NRPB) publication "Occupational Exposure to Electromagnetic fields: Practical Application of NRPB Guidance" NRPB-R301. This describes two mechanisms of interaction: induced currents and direct heating measured in terms of the SAR (specific energy
30 absorption rate). In general terms the induced current dominates

up to 2MHz above which the SAR effects take over.

According to a first aspect of the invention, there is provided an ingestible device as claimed in Claim 1.

5

This arrangement advantageously permits the use of an oscillating magnetic field as an external energy source for remotely triggering eg. the release of a compound from the capsule. For reasons discussed below, a magnetic field offers advantages over a field including radio waves.

10

Preferably the housing defined in Claim 1 is cylindrical. Other, non-circular section housings eg. polygonal cross sections are possible.

Preferably the dimensions of the coil are as defined in Claim 2. Such
15 dimensions advantageously permit the coil to form part of a capsule whose exterior is smooth and appropriately shaped and sized for ready ingestion. The use of an antenna as claimed is believed to obviate at least some of the space-inefficiency disadvantages of the Lambert *et al* capsule.

20 According to a second aspect of the invention there is provided an ingestible device as claimed in Claim 3.

The ferrite core and coil combination of the device of Claim 3 also allows, in an alternative embodiment of the invention, highly efficient
25 coupling of energy from a magnetic field to the circuitry forming part of the capsule. Thus this aspect of the invention allows the construction of an advantageously compact device whose energy efficiency is higher than that of prior art designs.

30 In preferred embodiments of the invention the receiver includes the ferrite

core and coil combination as one of its circuit components; either embodiment of the apparatus may optionally include a transmitter including a said air or ferrite core and coil combination.

5 The preferred operating regime for the device of the invention is between 1MHz and 14MHz. In addition to the biological effects there are a number of electromagnetic issues which influence the choice of operating frequency. One issue is restrictions on the use of the electromagnetic spectrum to prevent interference between various users. Thus 13.56MHz
10 is a preferred operating frequency as this frequency is designated for general industrial use. However, at this, the upper end, of the frequency range several adverse effects occur. These include loading of the transmitter by the body tissue, skin effect adversely affecting the receiver impedance and induction heating of metal objects.

15

The selected frequency for use of the preferred embodiment of the invention is therefore at the lower end of the range, nominally between 1 MHz and 3.0MHz.

20 The frequency effects therefore determine that the power transmitted to the device of the invention to energise the latch comes from a magnetic field of between 1.0MHz and 3.0MHz induced over the region of the body containing the capsule. The SSDC of the invention is designed with a means for extracting power from this magnetic field to energise the
25 latch. It should be noted that the magnetic field has no corresponding electric field such as in a radiowave and as such there is energy stored in the field with minimal loss until a receiver is placed within the field capable of extracting the energy.

30 The preferred embodiment of the receiver is a coil of wire arranged so

that the coil intercepts the field lines so that a voltage is induced across the coil by the time varying magnetic field. A capacitor connected across the coil tunes the circuit so that it has a resonant frequency equal to the frequency of the energising field. When such a tuned receiver is placed in
5 an oscillating magnetic field high currents are induced in the coil and this current generates a magnetic field of its own. It is the interaction of these fields which enables the receiver to extract significant amounts of real power from the energising magnetic field. This power can be accessed by connecting the latch electrical circuit in series or parallel with the
10 coil/capacitor tuned receiver.

The magnitude of the power that can be extracted from the magnetic field is a strong function of the size and shape of the antenna (receiver coil). The voltage induced in the coil is proportional to its area and the power
15 induced is proportional to the square of the voltage. Hence the power that can be extracted from the field is proportional to the fourth power of the diameter of the coil. In practice, the actual power is also modified by the permeability surrounding the coil and a shape factors relating to the length and the angular orientation of the coil to the field.

20

In a preferred embodiment of the invention an air cored design of receiver antenna has been developed which uses between 60 and 100 turns of copper wire in the range 0.1mm to 0.3mm diameter wound as a single or double layer cylindrical coil of diameter between 8mm and 12mm and
25 length between 10mm and 20mm.

Care must be taken in the design to minimise the effective impedance of the receiver coil in order to maximise the Q of the circuit. Unwanted impedance can be added to the circuit from a number of sources:

30

- Eddy currents in metallic components
- Skin depth effects in the conductor
- 5 - Dielectric loss in the tuning capacitor.

In addition the proximity of a conductive fluid to the coil can change the resonant frequency as it acts as an additional capacitance in parallel to the coil. It is therefore preferable to maintain a minimum separation of the
10 coil from any internal or external fluid. This distance should be in the range of 0.1mm to 1.0mm.

According to a third aspect of the invention there is provided an apparatus as defined in Claim 6. Further, advantageous features of this aspect of the
15 invention are defined in Claims 7 to 21.

More specifically, the preferred approach used in this invention is inductive coupling at a frequency which gives high energy density but at which the absorption by body tissue is small compared to the energy
20 coupled into the capsule. In this approach an alternating current is passed through one or more loops of a conductor such that an alternating magnetic field is generated between the loops. A preferred arrangement is to use two loops, one on either side of the abdomen. With this arrangement the amplitude of the magnetic field at any point between the
25 loops can be accurately controlled. Thus, for example, two loops separated by their radius form a Helmholtz pair giving a nominally uniform field over the full volume between the loops. In the invention the spacing between the loops would be between one radius and four radii. The preferred embodiment has a spacing between the loops equal to the
30 diameter of the loop as this maximises the central field value for a given

value of the reactive power of the field generator supply.

It should be noted that a coil pair will generate a combination of magnetic and electrostatic fields around it. The major one of interest is the
5 magnetic field which, in radio terms, only exists in the near field. The design of the field generator uses appropriate shielding to minimise the longer range radio waves and the electrostatic fields.

The energy that can be transmitted by an alternating magnetic field is a
10 function of its field strength, frequency and the mutual inductance between the energising and receiving coils. The apparatus of the invention optimises those three variables to meet the needs of safe and reliable operation with readily available electronic components.

15 The use of a pair of current loops to generate the field is chosen to maximise the magnetic field in the useful volume between the loops whilst minimising near field electric field and far field electromagnetic radiation. This minimises any potential effects on persons close to the field generator from the electric field gradient and also minimises stray electromagnetic
20 radiation which could interfere with other electrical equipment.

The maximum power level is achieved when the axis of the coil in the capsule is aligned with the axis of the coil of the external field generator. This cannot be guaranteed when the capsule is inside the GI tract.

25

In the prior art, arrangements have been made inside the capsule to ensure that the magnetic flux is guided through the receiver coil whatever the orientation. One example of this is the use of 3 orthogonal coils wound around a ferrite core with a 3 axis cross form, as disclosed in US-A-
30 5,167,626.

Within the size constraints of SSDC's such arrangements are sub-optimal in their efficiency in interacting with the external field as they suffer from poor shape factor. The preferred arrangement in this invention is the use of a single coil geometry which has high efficiency only when the external magnetic field is orientated along its preferred axis and to provide a means of changing the orientation of the energising field until it aligns with the capsule. Theoretically this can be achieved in a number of ways:

- 10 - Rotating the person with respect to the energising field
- Physically rotating the field generator with respect to the person
- Providing a plurality of energising coils at different angular
- 15 orientations and energising them sequentially or in combination to rotate the orientation of the magnetic field in space until it is aligned to the capsule axis.

The preferred embodiment of the invention uses 3 coil pairs mounted orthogonally to each other. The coils are sized to permit a person to be positioned within the space enclosed by the coils. An example of the typical size of the coils would be 600mm diameter and 600mm apart.

To facilitate entry of the person to the central region eg. the pair of coils with the vertical axis may be arranged so that part of the coils are contained on a door where continuity of the coil is provided by electrical connections on the door when it is closed; or the coils may be on a vertical slideway so that the person could stand at the correct location and the coils slid into position by moving vertically.

Another possibility is for the coil pairs to be supported on a wearable garment.

The energisation of the magnetic field generator requires powering the
5 field coils with current at the level necessary to generate the field at the required frequency of between 1.0MHz and 14.0MHz.

A typical field strength would be in the range 20Am^{-1} to 200Am^{-1} . To generate this field strength coils with multiple turns can be used where the
10 number of turns is chosen to match the capabilities of the electronic components driving the current. A preferred embodiment of the invention uses 2 turns per coil although other implementations may use from 1 to 10 turns per coil.

15 In order to minimise resistive heating at these frequencies large diameter conductors or Litz wire are preferred in the construction of the field coils, to minimise the effect of skin depth limiting current penetration into the wire.

20 The powering of the energising coils is traditionally accomplished using a circuit comprising a low power oscillator, an r.f. amplifier and a matching network to efficiently couple the coils to the amplifier. Typically the oscillator is crystal controlled for frequency stability. This approach suffers from the problem that changes to the load impedance can reduce
25 the field strength if the tuning of the matching unit becomes sub optimal due to, for example, the electrical effects of a body close to the coils.

In the apparatus of the invention the current is generated by using the field coils as part of the frequency determining components of a power
30 oscillator directly driving the coils. The major advantage of this approach

is that the field level remains constant even if the effective load impedance changes. This is achieved at the expense of a small change in frequency.

At the lower end of the preferred frequency range 1.0MHz to 3.0MHz the
5 frequency shift caused by the presence or absence of people or small metal objects within the energised field volume is small compared with the bandwidth of the tuned receiver in the capsule and hence there is minimal change in the receiver power. This is considered a major improvement on prior art as it provides more reliable actuation.

10

The power oscillator can be implemented using any of a range of established oscillator circuits. The preferred embodiment uses a Hartly oscillator and achieves efficient performance by the use of 6mm diameter copper tube for the coils and low dielectric loss capacitors for the passive
15 components and a low loss, high voltage power MOSFET for the active component.

According to a fourth aspect of the invention there is provided a method as claimed in Claim 23. Preferred features of the method are defined in
20 Claims 24 to 26.

It is desirable for an SSDC to indicate its location and status when in the GI tract. In particular it is important for the SSDC to indicate the precise moment at which the discharge of the substance from the reservoir occurs,
25 and for the SSDC to indicate its location in the GI tract at or close to such a time.

For this reason it is known to include in an SSDC a transmitter that transmits a signal, indicative of the status and, optionally, the location of
30 the SSDC, beyond the body of the mammal. One way of achieving the

latter effect is to provide a radiolabelled marker within the SSDC, that may be tracked within the GI tract by means of known Gamma scintigraphy techniques.

- 5 US-A-5,279,607 discloses an SSDC the operation of which is initiated by a receiver and latch combination. The receiver is a tuned resonant circuit, including a first antenna, that generates a current in a heating resistor when it couples, via the antenna, with an oscillating electromagnetic field of the same frequency as the resonant circuit, transmitted from outside the
10 body of the mammal.

The heating resistor is positioned to heat a fusible component that holds a resiliently deformable member in an energy storage (ie. high potential energy) condition. On fusing of the fusible component a diaphragm
15 moves and is ruptured by a pin. This causes two reagents to mix in a reaction chamber and generate a gas, the increasing pressure of which drives a piston to expel the substance from the reservoir of the SSDC.

The SSDC of US-A-5,279,607 includes a second resonant circuit capable
20 of acting as a transmitter of a signal intended to indicate emptying of the reservoir. The second circuit is initially isolated from the receiver circuit by an electrical short. A blade attached to the piston ruptures the short as it starts to move, thereby coupling the second resonant circuit to the electromagnetic field. This induces a current in the second circuit that is
25 transmitted, via a further antenna, for receipt and processing by a receiver external to the mammal.

The SSDC of US-A-5,279,607 suffers from the disadvantage that, because of the limited space within the capsule, the breakable short cannot
30 be placed anywhere other than close to the initial position of the piston -

otherwise the short may encroach into space intended for storage of the substance; or the blade may be unacceptably large compared with the other components in the capsule.

5 Consequently the blade in US-A-5,279,607 of necessity ruptures the short at the beginning of the travel of the piston. This means that the second resonant circuit may generate a signal indicative of discharge of the substance from the reservoir even when the SSDC fails to achieve this, eg. through sticking of the piston or failure of the gas generating reagents
10 to react completely.

Also if, as may be desirable or sometimes unavoidable in an SSDC, it is required to locate the second resonant circuit at a location spaced from the piston or other actuator that causes discharge of the substance, in the
15 SSDC of US-A-5,279,607 this may only be achieved at the expense of including comparatively long electrical connecting wires between the first circuit, the second circuit and the breakable short. This may complicate the process of assembly of the SSDC.

20 According to a fifth aspect of the invention there is provided a device as claimed in Claim 27.

The inclusion of a restraint advantageously permits limiting of the movement or extent of operation of the actuator mechanism.

25

The use of the restraint to operate the switch confers considerable design freedom on a designer of a device according to the invention. In particular, the switch may be located conveniently close to a transmitter circuit even if the latter is remote from the actuation mechanism.

30

Preferred features of the fifth aspect of the invention are defined in the claims depending from Claim 27.

There are various possible approaches to providing an on-board energy
5 source for the device 10.

In general terms to accomplish sufficient force and movement to expel the drug within a few seconds requires forces in the range 2 to 20N over distances of 2mm to 20mm. This typically amounts a mechanical power
10 level in the order of 0.1W or an energy of 0.1J. If the energy were stored in electrical form and used to drive an electromechanical actuator of simple form then typically the conversion efficiency would be less than 10%. An electrical energy storage system would then require to store 1J
15 of energy and deliver it at 1W power. Micro batteries as used in watches are of the necessary size and store easily sufficient energy; however they can only deliver that power at milliwatt rates. Capacitors however can deliver their energy at the required power levels but within the size constraint can only store milli Joules of energy.

20 Several other forms of energy storage are theoretically possible including

- Chemical gas generation
- Compressed nitrogen or air
- 25 - Liquified propellant fluids (eg. N₂O, butane/propane, HFA's)
- Springs
- 30 - Chemical heat generation

Chemical storage has potentially the highest energy density, but introduces issues associated with chemical compatibility, stability, triggering and toxicological safety.

5

Within the available space constraints there is sufficient volume to store the required energy either in springs or as a compressed gas, eg. air both of which forms are possible as the energy can be released directly in the desired form of a force acting to cause mechanical motion. However the
10 complexity of a device including a compressed air source may militate against its use.

According to a sixth aspect of the invention there is provided a device as claimed in Claim 33.

15

Another device according to a seventh aspect of the invention is defined in Claim 36; and a device according to an eighth aspect of the invention is disclosed in Claim 39.

20 Preferred features of the sixth, seventh and eighth aspects of the invention are defined in the claims depending from Claims 33, 36 and 39.

One preferred embodiment of the device includes a coil spring which operates to move a piston to expel the drug from inside the capsule
25 through an opening at the other end of the capsule. An example of the dimensions and components that could be used would be for a volume of 1ml available to contain the drug in the form of a cylinder 9mm in diameter and 16mm long. A coil spring of 8mm outer diameter compressed to a length of 4.6mm could exert an initial force of over 1kg
30 and have a residual force of 0.2kg after it has travelled the 16mm.

There now follows a description of preferred embodiments of the invention, by way of non-limiting example, with reference being made to the accompanying drawings in which:

5

Figure 1 is a perspective, partly sectioned view of an ingestible device according to the invention;

Figures 2a and 2b are, respectively, block diagram and schematic views of a receiver-transmitter circuit forming part of the Figure 1 device;

10 Figure 3 shows one embodiment of antenna for use in the Figure 1 device, including an antenna wire coiled about the capsule wall;

Figure 4 shows an alternative antenna, including an antenna wire coiled about a ferrite core within the device;

15 Figures 5a and 5b are, respectively, side elevational and plan views of an apparatus, according to the invention, for generating an oscillating, axial magnetic field;

Figure 6 shows, schematically, a preferred embodiment of oscillating field generator;

20 Figure 7 shows a further embodiment of oscillating field generator according to the invention;

Figures 8a and 8b are, respectively plan and cross-sectional views of a restraint and switch combination, according to the invention, before actuation of the switch;

25 Figures 9a and 9b are views, corresponding to the Figure 8 views, after actuation of the switch;

Figures 10 to 12 show three kinds of energy source in the form of compression springs; and

30 Figure 13 shows a restraining ring for retaining moveable components of the device of the invention within its housing, after dispensing of a substance.

Referring to the drawings there is shown an ingestible device 10 according to the invention.

5 The overall envelope of the device 10 has been designed to be compatible with swallowing and smooth passage through the GI tract. To support this requirement the outer housing 11 of device 10 is smooth with no sharp edges and preferably has at least one end rounded as shown at 11a to facilitate swallowing. The diameter of the capsule preferably does not
10 exceed 12mm and the length preferably does not exceed 35mm. The precise dimensions represent an optimisation between overall capsule size and the volume of a drug containing reservoir 12. In a preferred embodiment of the invention for a drug volume of 1.1ml the reservoir 12 has a diameter of 11mm and length 32mm. The end rounding 11a can
15 within the scope of the invention range between a hemispherical profile and a flat end with a 2mm radius corner.

Reservoir 12 has a cylindrical interior and is open at one end 13 located at the opposite end of device 10 to rounded end 11a. Before use of the
20 device 10 open end 13 of reservoir 12 is sealed against leakage of the contents of the hollow interior of reservoir by a closure member in the form of bung 14. Bung 14 is removable from open end 13, in a manner described below, to permit expulsion of the contents from the interior of reservoir 12. Thus if reservoir 12 is charged before insertion of bung 14
25 with a substance, which may be eg. in liquid or powder form, the substance may be released into the GI tract on operation of the device as described below.

The removal of bung 14, in use of the apparatus in the GI tract of a
30 mammal, from open end 13 is by virtue of selectively controlled

pressurising of the interior of reservoir 12.

This is achieved through the action of an actuator mechanism in the form of a cylindrical piston 16 that is sealingly slideable along the interior of
5 reservoir 12 under power from an energy source (eg. a stored energy device that is, for clarity, omitted from Figure 1).

The interior of device 10 on the side of piston 16 remote from reservoir
12 is generally hollow. Thus the energy source may in preferred
10 embodiments take the form of a compressed spring whose spring force acts between eg. the rear face of piston 16 and a shoulder defined by an annular or part-annular rib 17 that is integral with and hence fixed relative to the housing 11.

15 The hollow interior of device 10 includes a shaped space or recess 22 for receiving a radioisotope tag (not visible in the drawings) that may be used for tracking progress of the device 10 along the GI tract, eg. using *per se* known Gamma scintigraphy techniques.

20 The device 10 includes a releasable latch that operates to latch the energy source in a potential energy state until a chosen time.

In the Figure 1 embodiment the latch is in the form of an anchor 18, secured relative to piston 16, for a thread 19 made of or at least including
25 a sharp melting point material; and a heater 20 whose function is to heat the thread and melt it or at least cause a dramatic increase in its ductility at a chosen time.

More specifically, in the preferred embodiment anchor 18 includes a
30 tubular sleeve 21 one end face of which is rigidly secured to the rear face

16a of piston 16, such that the elongate axis of sleeve 21 is generally perpendicular to rear face 16a.

5 The hollow interior of sleeve 21 opens at the end of sleeve 21 remote from piston 16.

Sleeve 21 includes an elongate perforation 23, whose elongate axis is generally parallel to the elongate axis of sleeve 21, passing through the wall of sleeve 21 as shown. A similar perforation passes through the wall
10 of sleeve 21 on the opposite side thereof.

An elongate cylindrical anchor member 24 is slideably received at either end in the respective perforations, whereby the elongate axis of the anchor member is generally perpendicular to the elongate axis of the sleeve 21.
15

The diameter of anchor member 24 is less than the width of each perforation, whereby anchor member may be slid into place as shown during assembly of device 10.

20 Anchor member 24 has firmly secured thereto one end of thread 19. Thread 19 passes through the hollow interior of sleeve 21 and emerges at the free end thereof, from where it passes through an aperture 25b in a printed circuit board (pcb) 25. Pcb 25 is in the form of a disc secured against the side of annular rib 17 remote from reservoir 12. Thread 19 is
25 firmly secured to the surface 25a of pcb that is remote from reservoir 12. Surface 25a also mounts heater 20 in the form of a resistor. Thread 19 passes over heater 20 between the aperture and the attachment point of thread 19 to the pcb 25a.

30 If as disclosed hereinabove a compression spring (not shown in Figure 1)

acts between the rib 17 and piston 16, on assembly of device 10, sleeve 21 will be forced, by virtue of its attachment to piston 16, towards reservoir 12 until anchor member 18 engages the end of each perforation 23 remote from piston 16, causing thread 19 to become taut and thereby preventing the further travel of piston 16 towards bung 14 while thread 19 is intact. The tension in thread 19 draws pcb 25 hard against rib 17, thereby optionally obviating the need for further restraint of pcb 25.

Pcb 25 includes a tuned receiver of externally applied radiation whereby on the device passing through an electromagnetic field of the frequency to which the receiver is tuned, a current is induced that is fed to resistor heater 20. The heat from the heater 20 melts or renders highly ductile the thread 19, whereby piston 16 becomes free to move towards bung 14 powered by the energy stored in the spring.

Regardless of whether the substance in reservoir 12 is a liquid, a suspension, a solution a powder or even, in some embodiments of the invention, a solid, the action of piston pressurises the interior of reservoir 12 until bung 14 is forced partly or completely out of open end 13 of reservoir 13. The substance when in solid form may include, but is not limited to mini-tablets, pellets and cyclodextrin complexes, especially cyclodextrin complexes supporting further substances.

Since the interior of reservoir 12 is by then pressurised its contents are then expelled rapidly from within the device 10.

Thus if the electromagnetic field is applied when the device 10 is, following ingestion via the oesophagus, at a preferred location in the GI tract, site-specific drug delivery may be readily and rapidly achieved using a simple, reliable mechanism.

Figures 2a and 2b show the receiver and transmitter circuits 27, 28 of device 10 in more detail.

- 5 The receiver includes a coupling coil 29, described in more detail below, designed to couple as much energy as possible from a magnetic field incident on the device 10 while it is in the GI tract.

Coil 29 is connected to a tuner 30, that tunes the resonant frequency of the
10 receiver and includes one or more tuning capacitors C1, C2 connected in parallel in a *per se* known manner.

Tuner 30 is connected in series with resistor R₁ defining heater 20 that is mounted on the surface 25a of pcb 25, in contact with thread 19.

15

In the initial condition of the device 10 resistor R₁ is connected in series with the remainder of receiver circuit 27 by means of a short circuit line 32 including a breakable link 31.

- 20 Pcb 25 also includes a transmitter 28.

Transmitter 28 includes a rectifier 33 that rectifies the oscillating currents in receiver 27 when the transmitter becomes operational. Transmitter 28 includes a *per se* known Hartly oscillator including oscillator feedback
25 capacitor C₃; transmitter frequency determining capacitors C₄ and C₆; d.c. supply capacitor C₅; biasing resistors R₂, R₃ and R₄; and switching transistor Q₁. The outputs of the frequency determining parts C₄, C₆ of the oscillator are transmitted externally of the mammal by series antennae 34, 35. Transmitter 28 may optionally include a transmitter coil similar
30 to or constituted by coil 29.

Line 32 initially isolates transmitter from any current induced in receiver 27, until breakable line 31 is broken in a manner described below. At that point direct current, rectified by rectifier 33, flows in transmitter 28 and produces an oscillating output by virtue of the presence of the Hartly oscillator circuit.

The values of receiver tuning capacitors C_1 and C_2 and the oscillator frequency determining capacitors C_4 and C_6 are chosen so that the resonant frequency of receiver circuit 30 is distinct from the output frequency of the transmitter 28, thereby avoiding confusion between the fields input to and output by the device 10.

Referring now to Figure 3, one arrangement of the receiver coupling coil 29 is shown, in which the coiled antenna wire 29 is embedded in the cylindrical outer wall of the housing 11 of the device 10. This arrangement is advantageously space-efficient and provides an air core for the wire 29.

In the preferred embodiment of the invention the diameter of the coil defined by wire 29 is 8-12mm; and the length l from one end to the other of the coil is 10-20mm. The preferred wire diameter is 0.1mm-0.3mm and the antenna coil preferably has 60-100 turns.

Figure 4 shows an alternative embodiment of the device 10 of the invention, in which the receiver coil 29a includes a ferrite core 36.

The ferrite core and coil form a central axial rod rigidly connecting the two discs 16a, 16b to define a bobbin-like member. The discs 16a, 16b have sliding seals 16c that slide along the hollow interior of the capsule

body. The space between the discs 16a, 16b forms the reservoir 12 for the substance 12a to be dispensed. The disc 16a adjacent to the pcb 25 acts as the piston and the disc 16b at the other end acts as a cap. A compression spring 50 acts between pcb 25 and disc 16a and tends to
5 drive the bobbin-like structure out of the openable end 11a of the housing 11. A latch and actuator mechanism similar to those of Figure 1 temporarily prevent expulsion of the bobbin-like structure and hence the substance 12a, in a manner similar to that described hereinabove in relation to Figure 1.

10

The tuning components and the latch mechanism are mounted on the bobbin separated from the substance to be released by the lower disc and seal or may be on the capsule body 11 and connected to the bobbin by fine wires. After the latch is activated and the spring 50 is released the whole
15 of the bobbin is slid out of the open capsule end. This avoids the need to pressurise the capsule to push off the cap.

Since the ferrite core 36 couples the magnetic flux more efficiently than the air core shown in Figure 3, the coil 29a in Figure 4 can be made of
20 smaller diameter than the Figure 3 coil. Consequently the ferrite-cored coil 29a may be located as a discrete component within housing 11, as shown.

Regardless of the precise design of the coil 29, the loops thereof
25 preferably are spaced from any fluid within or surrounding the device by a distance of 0.1mm to 1mm. This minimises the capacitance effects of neighbouring fluids while maintaining compactness of the device 10. The ferrite core (when present) may be similarly isolated from fluids. The isolation may arise because of a coating on the outer surface of the
30 coil/core combination 29a, 36 of Figure 4.

In the Figure 4 embodiment the ferrite core 36 includes an axial bore. The thread 19 extends along the bore and is anchored as shown to disc 16b.

5

Figures 5a and 5b show a simplified form of an external field generator 40 according to the invention for transmitting power to a device such as, but not limited to, device 10 of Figure 1.

10 The field generator 40 includes a support in the form of a box-like housing 41 for each of a pair of field coils 42.

The pair of coils 42 are in juxtaposition to one another and preferably but not essentially are dimensioned to define a Helmholtz pair. The location
15 of and the spacing between the coils are such that, on positioning of a mammal between the coils, the coils lie on opposite sides of the abdomen of the mammal.

The coils 42 are each connected to a source of oscillating electrical energy
20 in the form of oscillator 43.

Thus a device 10 in the GI tract can be activated by the field generator 40 when the abdomen of the mammal is between the juxtaposed coils 42 and the oscillator switched on.

25

The radius r of each coil 42 is the same in the preferred embodiment shown. The spacing s between the coils is between one and four times, and especially twice, the radius r . In the Figure 5 embodiment $s \approx 500\text{mm}$, but other embodiments in which $400 < s < 800\text{mm}$ are believed
30 to offer good field generation while providing sufficient space between the

coils 42 to accommodate the mammal. Obviously when the spacing s does not equal the radius r , the coils do not function as a Helmholtz pair.

The foregoing features confer advantages as disclosed hereinabove.

5

As noted hereinabove, the field generator 43 preferably generates a field that oscillates in the frequency range 1MHz-14MHz, and more preferably in the range 1MHz-3MHz.

- 10 The field coils generate, *inter alia*, a near field magnetic field. This has a large energy content which is continually being exchanged between the field and the current in the coils. As such no power is being used up to maintain this field, apart from resistive losses, until the receiver coil interacts with the field to extract energy. In this way the systems is like
15 an air cored transformer rather than a radio transmitter.

- The housings 41 for the coils 42 optionally include shielding. The function of the shielding is to provide a primary safety earth screen around the field coils to protect persons touching any exposed conductors
20 resulting from mechanical damage to the insulation. The shielding is such as to avoid forming closed loops through which the field passes as these will induce current flow and reduce the field levels generated by the coils.

- The shielding may also be used to reduce the magnitude of the electric
25 field outside of the shielding generated by the coils and also the radio wave that is generated along with the magnetic field. This is advantageous in reducing any effect on other electronic equipment in the vicinity of the device. Should additional shielding be required then the coils, the oscillator and the user of the capsule could all be contained
30 within an earthed mesh containment room or cubicle.

Referring now to Figure 6 there is shown a further, and presently more preferred, embodiment of field generator 40 in which there are three pairs of the field coils 42. In Figure 6 the pairs are arranged to generate three
5 mutually skewed, and, more particularly, mutually orthogonal, oscillating magnetic fields, by virtue of arrangement of the coils as faces of a cube.

The pairs of coils are in Figure 6 labelled according to the following key:

Coil	Cube Face
$C_{z1} + C_{z2}$	top and bottom faces
$C_{x1} + C_{x2}$	side faces
$C_{y1} + C_{y2}$	front and back faces

10

To enable a person to stand within the coils a spacing s between juxtaposed coils 42 of between 400mm and 800mm is appropriate.

In the Figure 6 embodiment the respective coils 42 may if desired be
15 secured in a framework, that may also if desired support the shielding visible in Figure 5, whereby a mammal may stand, sit or lie in the region between the coils.

The framework may support at least one of the coils in a moveable
20 fashion (eg. in a removable or hinged door or panel). This facilitates access to the inter-coil space, and in some embodiments permits adjustment of the spacing between the coils 42.

The framework is omitted from Figure 6 for clarity.

25

In Figure 7 there is shown another arrangement of the coils 42. In Figure

7 the components are functionally similar to their counterparts in Figure 6, but the coils of pair C_{z1} , C_{z2} are formed as flat circular coils, whereas the coils C_{x1} , C_{x2} , C_{y1} and C_{y2} define arcuate planes that confer on the coil array as a whole a hollow cylindrical shape. This arrangement of coils
5 may be supported on a frame as in the Figure 6 embodiment; or they may if desired be supported on a wearable garment 41a schematically illustrated by dotted lines in Figure 7.

Regardless of the precise arrangement of the coils the embodiments of
10 Figures 6 and 7 generate three mutually orthogonal, oscillating magnetic fields the flux lines of at least one of which will intersect the antenna 29 of the device 10, regardless of the orientation of the device 10 in the GI tract. Thus the energy in the magnetic field is efficiently transmitted to the device 10 to power its operation.

15

The coils 42 in the preferred embodiments each include eg. 1-4 turns of a large diameter (6mm diameter) hollow copper conductor with a wall thickness of 1mm.

20 Figures 8 and 9 show a mechanism, in accordance with the invention, for initiating transmission of a signal, by transmitter 28, indicative of discharge of the substance from reservoir 12 into the GI tract.

Figures 8 and 9 show some of the components of device 10 (with others
25 removed for clarity) in the vicinity of piston 16 and pcb 25.

Figures 8 and 9 schematically show the spring 50 (not visible in Figures 1 and 2), that acts between rib 17 and the rear face 16a of piston 16 to provide an on-board energy source for powering movement of piston 16,
30 in respectively its compressed (Figure 8) and uncompressed (Figure 9)

condition.

Sharp phase change thread 19 and heater resistor 20, forming part of the thermally actuated latch arrangement visible in Figure 1, are omitted from
5 Figures 8 and 9. However, the effect of delatching of the latch is evident in these figures in the release of the spring 50 to drive the piston 16.

A restraint in the form of a further, essentially non-fusible thread 51 interconnects rear face 16a of piston 16 and rear face 25a of pcb 25, by
10 passing through central aperture 25b of pcb 25.

Non-fusible thread 51, on exiting aperture 25b on rear face 25, is looped through the wire defining breakable link 31 shown schematically in Figure 2. Non-fusible thread 51 is firmly anchored to rear face 25a at a location
15 52 spaced laterally from breakable link 31.

When thread 19, which may also pass through aperture 25b as shown in Figure 1, is taut as shown in Figure 1, non-fusible thread 51 is loose as a result of being significantly longer than thread 19.
20

When thread 19 fuses and releases the energy in spring 50, thread 51 rapidly tightens. As it does so it moves laterally in the vicinity of breakable link 31 so that it instantaneously ruptures link 31 to form unconnected link parts 31a and 31b (Figure 9a). This connects the
25 transmitter and receiver circuits together as previously described, so that the device 10 emits a signal indicative of expulsion of the substance from reservoir 12.

The amount of slack in thread 51 in the pre-expulsion condition (Figure 8)
30 is adjustable by choosing the length of thread 51. Thus the precise

moment of rupturing of link 31, corresponding to a chosen point in the travel of piston 16, is adjustable.

5 The thread 51 may also serve as a limit or restraint to movement of the piston 16, in the sense that when thread 51 tightens as shown in Figure 9 it prevents further movement of piston 16. This ensures that piston 16 and spring 50 are retained within device 10 even after expulsion of the substance.

10 Where thread 51 is used to both rupture the link and restrain the piston a means is required to set the amount of movement of the piston which causes the link to rupture. This may be achieved by positioning the link so that as the thread tightens the force is applied at the appropriate time or by attaching the thread to the link with adhesive at the appropriate
15 location. It may also be preferable to use a restraining thread which has a higher temperature tolerance than the latch thread to ensure that even if the device is kept in a high field environment for a long time after operating there is no possibility that the restraining thread could be broken by the temperatures reached. A suitable thread could be made from
20 materials such as kevlar, tungsten or carbon fibre.

An alternative restraint for the moveable parts, of device 10, is shown in Figure 13.

25 Figure 13 shows a portion of the housing 11 of the Figure 3 device 10 (having an air cored coil). The piston 16 is visible at the end of its travel, following expulsion of the substance 12a from within the reservoir 12.

A restraining ring 75 is secured on an inwardly directed shoulder 76.
30 formed in the inner wall of housing 11 a short distance from the open end

13 of device 10. Ring 75 effectively reduces the diameter of the interior of housing 11, near to open end 13, to the extent that piston 16 is retained within reservoir 12 after use of the device 10.

5 The edge 75a of ring 75 facing piston 16 is chamfered to reduce the impact force arising from contact of the piston 16 and ring 75. The chamfer shown at 75a also applies both axial and radial forces to the piston 16.

10 The ring 75 may be manufactured from the same material as housing 11, in which case ring 75 may be welded, eg. using a solvent welding technique, to the housing 11.

When the material of ring 75 differs from that of housing 11, glue
15 bonding may be used instead to secure the ring in place.

As noted hereinabove, when the energy source is configured as a spring, it is desirable that the spring force is linear for as much of its travel as possible.

20

The requirement is also to achieve a specific force profile using a compression spring which cannot exceed given dimensions, as follows:

Force Profile

25

Force at full compression sufficient
to unstick piston

> 10N to 30N

Force after 10mm travel sufficient to

30 remove the bung 14

> 5N to 15N

Space Constraints

Outer diameter < 9mm

5

Inner diameter > 4mm

Length (as small as possible) < 6mm

10 A number of approaches have been identified:

1) Single Compression Spring as shown in Figure 10

15 A *per se* single coil spring as shown in Figure 10a may not utilise the available space efficiently, as only the outer annulus can be used.

20 As the spring only has to work once in the device 10 it can be designed with its stress load close to its yield point. The preferred spring therefore has a higher than usual helical angle and thicker wire size than available in standard springs. The Figure 10b spring 50, according to the invention, has a helical angle α_2 of 15° and a wire thickness t of 0.8mm. As illustrated the angle α_2 in the Figure 10b spring is greater than the helical angle α_1 of the Figure 25 10a spring.

2. Two Concentric Compression Springs as shown in Figures 11a (elevational view) and 11b (plan view)

Two compression springs 50a, 50b with one inside the other makes better use of the available space. The spring diameters need to be chosen to ensure free movement relative to each other and the neighbouring parts of device 10. If the clearance is small then winding one coil clockwise and the other anti-clockwise will reduce the risk of adverse interaction between them. Spring 50a is in Figure 11 wound clockwise and spring 50b is wound anticlockwise for this reason. Where sufficient clearance is available springs wound in the same direction could be used. This permits the use of standard springs rather than custom ones.

3. Wavy Springs as shown in Figures 12a and 12b

Thin washers 55 plastically deformed in circumferential waves act as compression springs. Multiple washers 55 welded peak to trough as shown can give the required extension.

Performance can be superior to a coil spring in this application as more of the available space can be utilised. Thus, for example, a 0.25mm thick annular washer with o.d. 8.5mm and i.d. 4.5mm could be formed to have 3 circumferential waves with a peak to peak height of 2mm. Welding 16 of these together at their peaks forms a wavy spring with a compressed length of 4mm, an extended length of 32mm and a force profile superior to a coil spring in the available space.

Figure 12a shows such a spring in the uncompressed state; and

Figure 12b shows the spring when it is compressed, prior to expulsion of the substance 12a from the reservoir 12.

5 In use of the device 10 the reservoir 12 is charged with a substance to be released and the latch set. These steps can take place during or after manufacture of the device 10, depending on the precise design of the device and its intended use.

10 Following such preparation the device 10 is ingested by a mammal under investigation and its progress along the GI tract monitored, eg. using a tracking technique as disclosed herein. When the device 10 reaches a chosen location in the GI tract an apparatus such as that shown in Figures 5, 6 or 7 is operated to activate the device 10. The device 10 expels the substance 12a from reservoir 12 and the transmitter sends a signal that
15 may be detected and processed as desired by external circuitry.

The substance 12a typically may be a pharmaceutical whose efficacy at the chosen GI tract site is under investigation. Alternatively, in uses of the apparatus not forming part of the invention as claimed, the substance
20 12a may be a therapeutic or diagnostic agent.

CLAIMS

1. An ingestible device for delivering a substance to a chosen or identifiable location in the alimentary canal of a human or animal,
5 comprising
an openable reservoir, for the substance, that is sealable against leakage of the substance;
an actuator mechanism for opening the reservoir;
an energy source, operatively connected for powering the actuator
10 mechanism;
a releasable latch for controllably switching the application of power to the actuator from the energy source; and
a receiver of electromagnetic radiation, for operating the latch when the receiver detects radiation within a predetermined characteristic
15 range, the receiver including an air core having coiled therearound a wire; characterised in that the coiled wire lies on or is embedded in an outer, wall of the device.
2. A device according to Claim 1 wherein the diameter of the coils of
20 the wire is in the range 8-12mm and its length is in the range 10-20mm.
3. An ingestible device for delivering a substance to a chosen or identifiable location in the alimentary canal of a human or animal, comprising
25 an openable reservoir, for the substance, that is sealable against leakage of the substance;
an actuator mechanism for opening the reservoir;
an energy source, operatively connected for powering the actuator mechanism;
30 a releasable latch for controllably switching the application of

power to the actuator from the energy source; and

a receiver of electromagnetic radiation, for operating the latch when the receiver detects radiation within a predetermined characteristic range, the device including a ferrite core having coiled therearound a coiled wire for coupling received electromagnetic radiation to the releasable latch, characterised in that the device comprises an elongate, hollow housing, the ferrite core being elongate with its longitudinal axis aligned with the longitudinal axis of the hollow housing.

4. A device according to any of Claims 1 to 3, wherein the receiver includes the said ferrite core and coil.

5. A device according to any preceding claim, wherein the ferrite core and coil are spaced from any fluid within or outside the device by a distance of 0.1mm to 1mm.

6. A device according to any preceding claim, including a transmitter having an air or ferrite core having coiled therearound a wire for transmitting electromagnetic radiation.

7. An apparatus for transmitting electromagnetic radiation to power an ingestible device, the apparatus comprising:

a support supporting a pair of transmitter coils operatively connectable to a source of oscillating electrical current, the support supporting the respective coils of the pair on opposite sides of the abdomen of an animal.

8. An apparatus according to Claim 7 wherein the coils define a Helmholtz pair.

9. An apparatus according to Claim 7, wherein the loops of the pair of coils are each of generally the same radius and are spaced from one another by between one and four times the said radius.
- 5 10. An apparatus according to Claim 9, wherein the loops are spaced from one another by twice the said radius.
11. An apparatus according to Claim 9 or Claim 10, wherein the spacing between the loops lies in the range 400mm – 800mm.
- 10 12. An apparatus according to any of Claims 7 to 11 including three said coil pairs supported on the support whereby to provide three mutually skewed fields.
- 15 13. An apparatus according to Claim 12 wherein the coil pairs provide three mutually orthogonal fields.
14. An apparatus according to any of Claims 7 to 13 wherein the frequency of the oscillating field generated by the or each coil pair is in
20 the range 1MHz – 14MHz.
15. An apparatus according to Claim 14 wherein the said frequency is in the range 1MHz – 3MHz.
- 25 16. An apparatus according to any of Claims 7 to 15 including shielding that inhibits the transmission of short wave electrostatic radiation.
- 30 17. An apparatus according to any of Claims 7 to 16 including shielding that inhibits the transmission of long wave radio waves.

18. An apparatus according to any of Claims 7 to 17 wherein the support is or includes a wearable garment.
- 5 19. An apparatus according to any of Claims 7 to 17 wherein the support includes a framework supporting one or more of the coil pairs, the framework permitting the abdomen of a mammal to intercept the magnetic field from the or each Helmholtz pair.
- 10 20. An apparatus according to Claim 19 wherein the framework includes at least one releasably securable member supporting a said loop, thereby permitting a mammal to enter and leave the vicinity of the or each magnetic field.
- 15 21. An apparatus according to any of Claims 7 to 20 wherein the spacing between the or at least one said pair of loops is adjustable.
22. An apparatus according to any of Claims 7 to 21 wherein the size and/or position of the field coils of the or at least one said coil pair
20 determine the frequency of oscillation of the magnetic field generated thereby.
23. An apparatus according to any of Claims 7 to 20 wherein each loop of a said coil pair includes between 1 and 10 turns.
- 25 24. An apparatus according to any of Claims 7 to 23 wherein each loop defines at least part of the frequency determining stage of a power oscillator.
- 30 25. A method of operating an ingestible device for delivering a

substance to a chosen or identifiable location in the alimentary canal of a human or animal, comprising

an openable reservoir, for the substance, that is sealable against leakage of the substance;

5 an actuator mechanism for opening the reservoir;

an energy source, operatively connected for powering the actuator mechanism;

a releasable latch for controllably switching the application of power to the actuator from the energy source; and

10 a receiver of electromagnetic radiation, for operating the latch when the receiver detects radiation within a predetermined characteristic range; the receiver being capable of extracting energy from an oscillating magnetic field and the method comprising:

causing a mammal to ingest the ingestible device;

15 at a chosen time, generating at least one axial, oscillating magnetic field and directing the field at the abdomen of the mammal whereby the receiver intercepts the said field and triggers the latch to cause opening of the reservoir; and

simultaneously inhibiting the generation of long wave radio waves
20 and short wave electrostatic radiation in the vicinity of the said abdomen.

26. A method according to Claim 25 including the step of generating two or more axial, oscillating magnetic fields whose axes are mutually skewed.

25

27. A method according to Claim 26 including the step of generating three said fields, wherein the axes of the said fields are mutually orthogonal.

30 28. A method according to any of Claims 25 to 27 wherein the or each

said field is generated using a coil pair operatively connected to a source of an oscillating current.

29. An ingestible device for delivering a substance to a chosen or
5 identifiable location in the alimentary canal of a human or animal,
comprising

an openable reservoir, for the substance, that is sealable against
leakage of the substance;

an actuator mechanism for opening the reservoir;

10 an energy source, operatively connected for powering the actuator
mechanism;

a releasable latch for controllably switching the application of
power to the actuator from the energy source;

a receiver of electromagnetic radiation, for operating the latch
15 when the receiver detects radiation within a predetermined characteristic
range; and

a transmitter of electromagnetic radiation for transmitting a signal
indicative of operation of the device,

the said reservoir including an exit aperture, for the substance,
20 closed by a closure member sealingly retained relative to the aperture by a
latch; wherein:

(i) the latch is thermally actuated;

(ii) the energy source is held in a potential energy state by the
latch until the latch operates; and

25 (iii) the device includes a heater for heating the latch whereby,
on the receiver detecting the said radiation the receiver operates to power
the heater and thereby release the latch, permitting expulsion of the
substance from the reservoir; characterised in that:

the device also includes a restraint operable to limit operation of the
30 actuator mechanism; and in that, on release of the latch, the restraint

operates a switch to activate the transmitter for transmission of a said signal.

30. A device according to Claim 29 wherein:

5 the actuator mechanism includes a moveable member moveable under power of kinetic energy from the energy source to promote expulsion of the substance from the reservoir;

the restraint includes a flexible member interconnecting the moveable member and an anchorage fixed relative to the remainder of the
10 device; and

the switch includes a breakable, electrically conductive member, the flexible member and the breakable member being mutually engageable whereby on movement of the moveable member sufficiently partly or completely to expel or initiate expulsion of the substance from the
15 reservoir the flexible member engages and breaks the breakable member to operate the switch.

31. A device according to Claim 29 or Claim 30 wherein the transmitter includes a resonant circuit connectable to draw power from the
20 receiver; and the breakable member is an electrical short that electrically isolates the resonant circuit from the receiver until the flexible member breaks the breakable member.

32. A device according to any of Claims 29 to 31 wherein the length of
25 the flexible member is such as to limit the travel of the moveable member to a chosen maximum.

33. A device according to any of Claims 29 to 32 wherein the restraint and the switch are so dimensioned and/or located that the restraint
30 operates the switch at a time corresponding to a predetermined amount of

movement of the moveable member.

34. An ingestible device for delivering a substance to a chosen or identifiable location in the alimentary canal of a human or animal,

5 comprising

an openable reservoir, for the substance, that is sealable against leakage of the substance;

an actuator mechanism for opening the reservoir;

an energy source, operatively connected for powering the actuator
10 mechanism;

a releasable latch for controllably switching the application of power to the actuator from the energy source; and

a receiver of electromagnetic radiation, for operating the latch when the receiver detects radiation within a predetermined characteristic
15 range;

the energy source including a compressed spring the expansion of which is initiatable by the latch and the work of the expansion of which causes operation of the actuator mechanism, characterised in that the spring, in its uncompressed state, has a minimum helical angle of 15°.

20

35. A device according to Claim 34 wherein the spring includes a wire whose diameter is approximately 0.8mm.

36. A device according to Claim 34 or Claim 35 wherein the spring
25 defines a hollow cylinder.

37. An ingestible device for delivering a substance to a chosen or identifiable location in the alimentary canal of a human or animal, comprising

30 an openable reservoir, for the substance, that is sealable against

leakage of the substance;

an actuator mechanism for opening the reservoir;

an energy source, operatively connected for powering the actuator mechanism;

5 a releasable latch for controllably switching the application of power to the actuator from the energy source; and

a receiver of electromagnetic radiation, for operating the latch when the receiver detects radiation within a predetermined characteristic range;

10 the energy source including a compressed spring the expansion of which is initiatable by the latch and the work of the expansion of which causes operation of the actuator mechanism, characterised in that the spring includes a pair of wires each coiled in loops to define a pair of hollow cylinder-like shapes, a first said cylinder-like shape being of a
15 greater internal diameter than the outer diameter of the second said cylinder-like shape and the first cylinder-like shape encircling the second cylinder.

38. A device according to Claim 37 wherein the wire of the first
20 cylinder-like shape is looped in a clockwise direction and the wire of the second cylinder-like shape is looped in an anticlockwise direction; or *vice versa*.

39. A device according to Claim 37 or Claim 38 wherein the first and
25 second cylinder-like shapes are spaced from one another in the radial direction of the spring cross section.

40. An ingestible device for delivering a substance to a chosen or identifiable location in the alimentary canal of a human or animal,
30 comprising

an openable reservoir, for the substance, that is sealable against leakage of the substance;

an actuator mechanism for opening the reservoir;

an energy source, operatively connected for powering the actuator
5 mechanism;

a releasable latch for controllably switching the application of power to the actuator from the energy source; and

a receiver of electromagnetic radiation, for operating the latch when the receiver detects radiation within a predetermined characteristic
10 range;

the energy source including a compressed spring the expansion of which is initiatable by the latch and the work of the expansion of which causes operation of the actuator mechanism, characterised in that the spring comprises a stack of resiliently deformable discs, the periphery of
15 each disc having formed therein a series of waves, the waves of respective said discs connecting such that the peak of each wave contacts the trough of a wave of an adjacent said disc.

41. A device according to Claim 40 wherein the waves of each disc
20 radiate generally from its centre.

42. A device according to Claim 40 or Claim 41 wherein each disc is an annulus.

25 43. A device according to Claim 42 wherein each annulus is about 0.25mm thick and has three said waves, the peak to trough distance of the waves being about 2mm.

44. A device according to Claim 43 wherein the spring includes 16 said
30 annuli secured together at the respective peaks and troughs of the waves.

45. A device according to Claim 42 or any claim dependent therefrom, wherein the outer diameter of each annulus is about 8.5mm and the inner diameter is about 4.5mm.

5

46. A device according to any of Claims 34 to 45 wherein the actuator mechanism includes a piston moveable under power from the spring for compressing the substance in the reservoir to promote its expulsion therefrom, the spring being secured at one end directly or indirectly to the
10 piston and at its other end to a member fixed relative to the remainder of the device.

47. A device according to Claim 46 when dependent from Claim 36, Claim 37 or Claim 42 wherein the spring encircles one or more further
15 components of the device.

48. A device according to any of Claims 1 to 6 or 29 to 47 including a retainer for retaining moveable components within the device.

20 49. A device according to Claim 48 wherein the retainer includes a rib that reduces the cross sectional area of the hollow interior of the device in the vicinity of an opening therein.

50. A device according to any of Claims 1 to 6 or 29 to 49 the
25 reservoir of which includes a charge of liquid, powdered or solid substance or a suspension or solution for discharge into the GI tract of a mammal.

51. A device according to any of Claims 1 to 5 or 29 to 50, including a
30 radioisotope tag generating radiation that is detectable for indicating the

location of the device in the GI tract of a mammal.

52. A method according to any of Claims 23 to 26, including the step of indicating the location of the device in the GI tract of the mammal,
5 using a radioisotope tag.

53. A method according to Claim 52 wherein the step of indicating the location includes using Gamma scintigraphy to indicate the location of the device in the said GI tract.

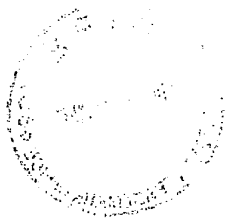
10

54. A device generally as herein described, with reference to and or as illustrated in Figures 1 to 4 and 8 to 12 of the accompanying drawings.

55. A method generally as herein described.

15

56. Apparatus generally as herein described, with reference to and or as illustrated in Figures 5 to 7 of the accompanying drawings.



ABSTRACT
AN INGESTIBLE DEVICE

5 An ingestible device (10) for delivering a substance (12a) to a chosen
location in the GI tract of a mammal includes a receiver of
electromagnetic radiation for powering an openable part of the device (10)
to an opened position for dispensing of the substance (12a). The receiver
includes a coiled wire 29 that couples the energy field, the wire 29 having
10 an air or ferrite (36) core.

In a further embodiment the invention includes an apparatus for
generating the electromagnetic radiation, the apparatus including one or
more pairs of field coils (42) supported in a housing.

15

The device (10) optionally includes a latch defined by a heating resistor
(20) and a fusible restraint (19). The device (10) may also include a
flexible member (51) that may serve one or both the functions of
activating a transmitter circuit (28) to indicate dispensing of the substance;
20 and restraining of a piston (16) used for expelling the substance.

(Figure 1)

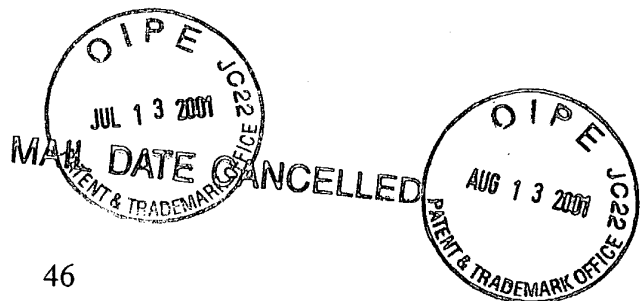
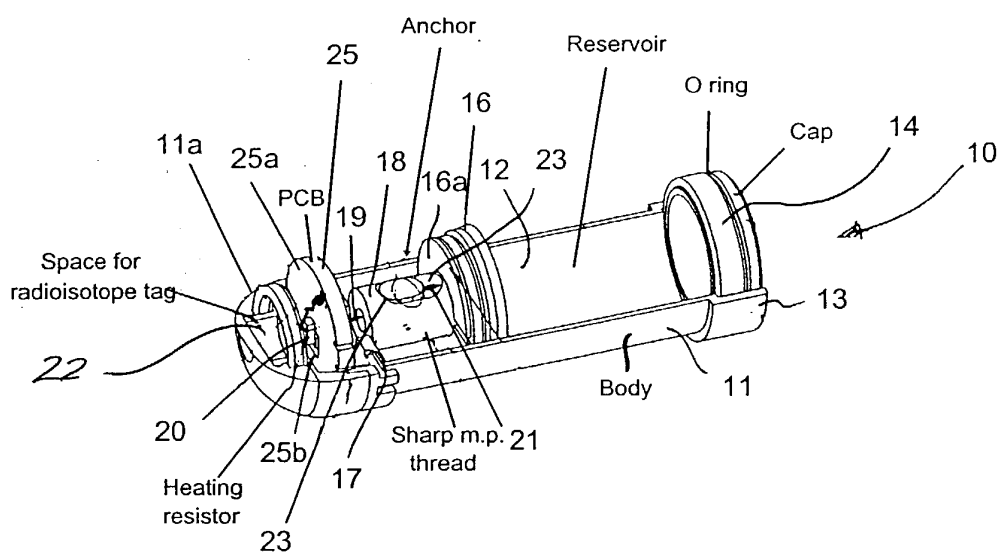


FIGURE 1



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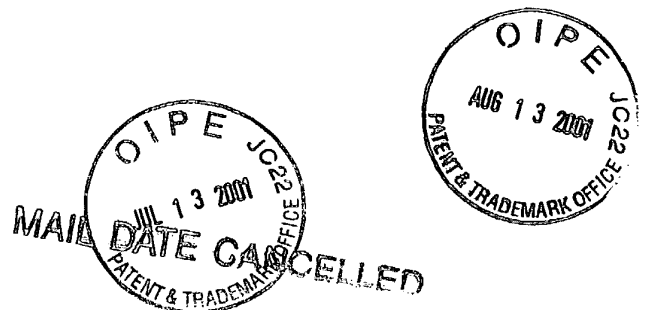
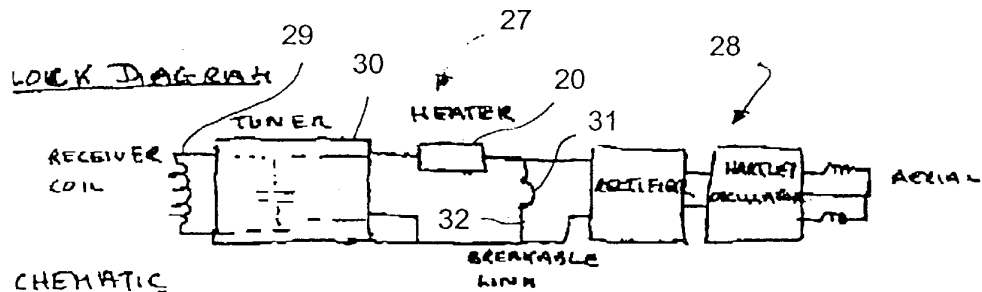


FIGURE 2a



CHEMATIC

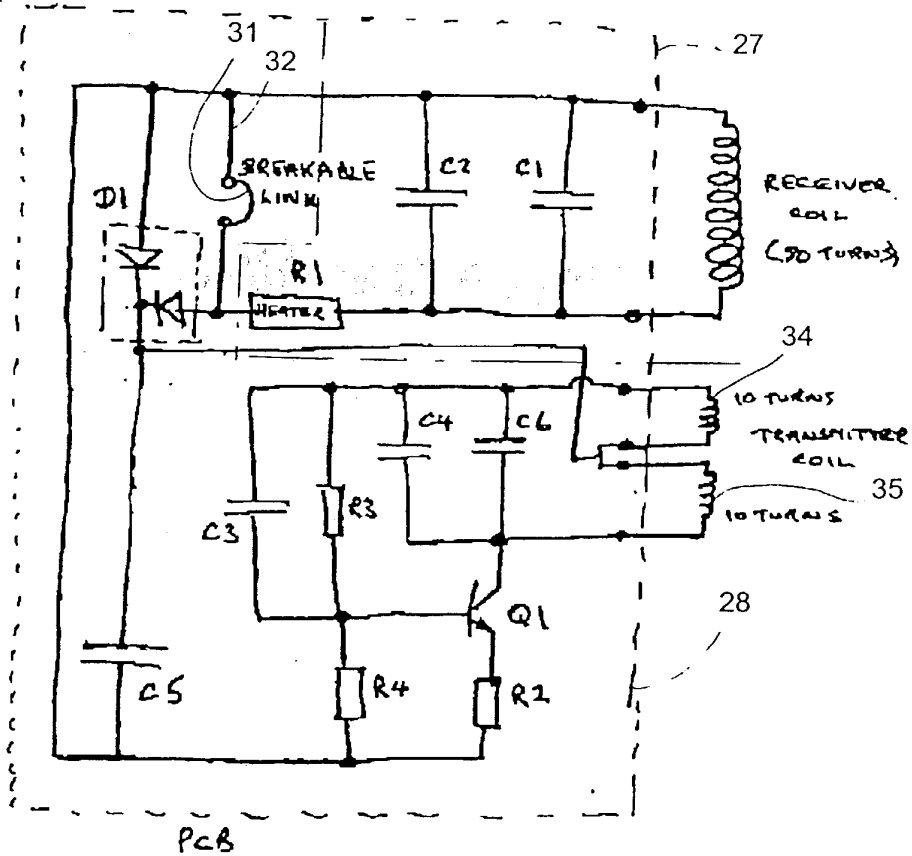


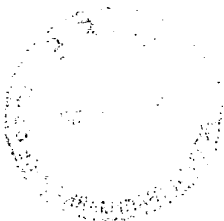
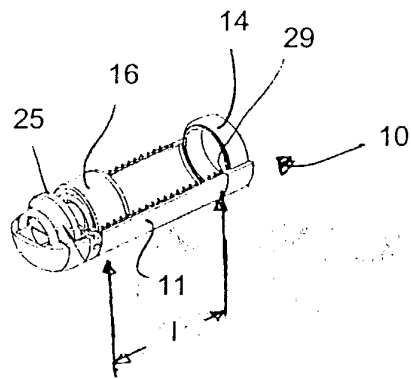
FIGURE 2b



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FIGURE 3



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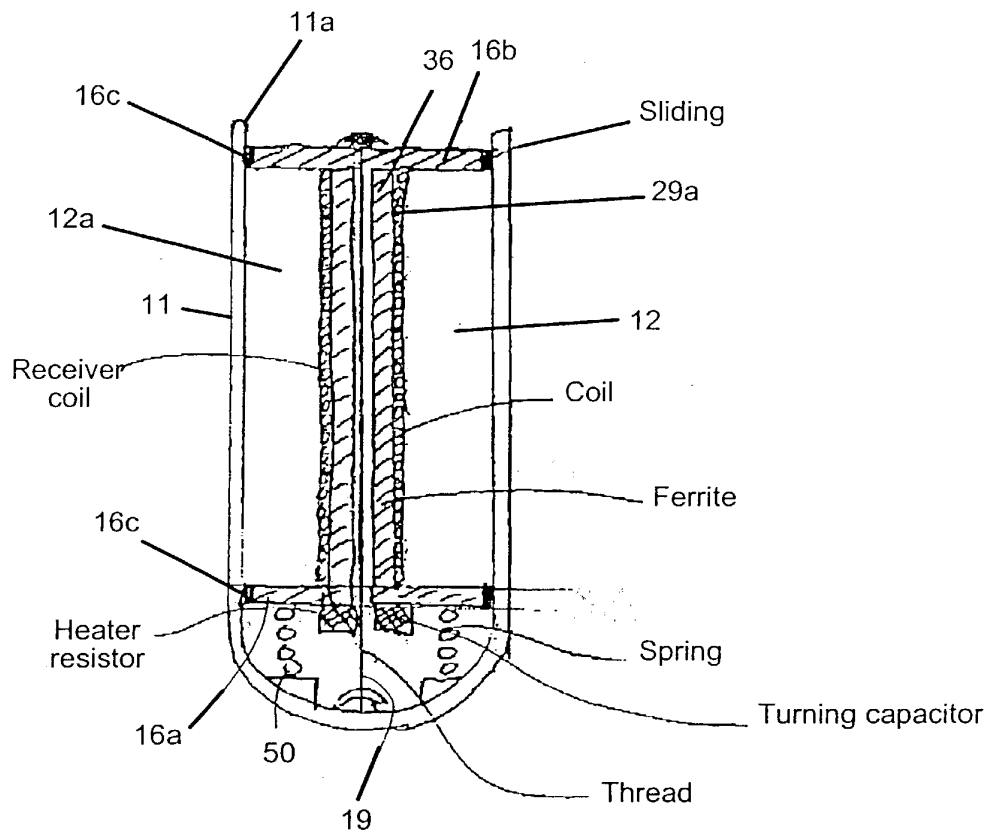


Figure 4

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FIGURE 5a

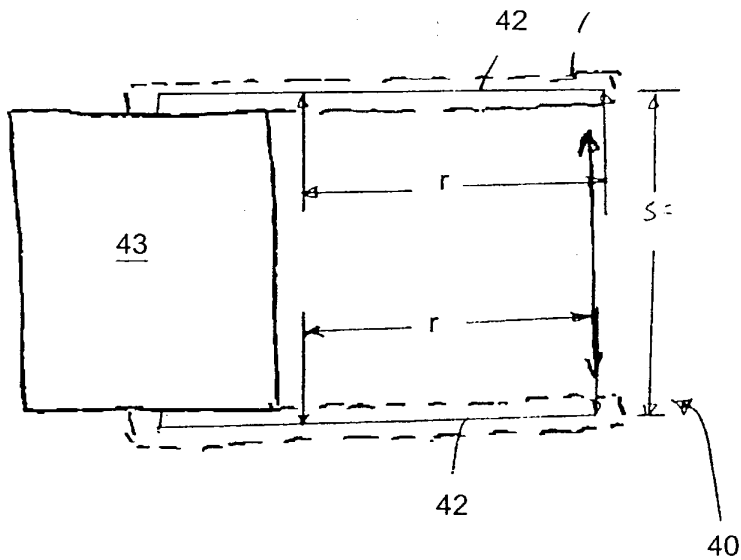
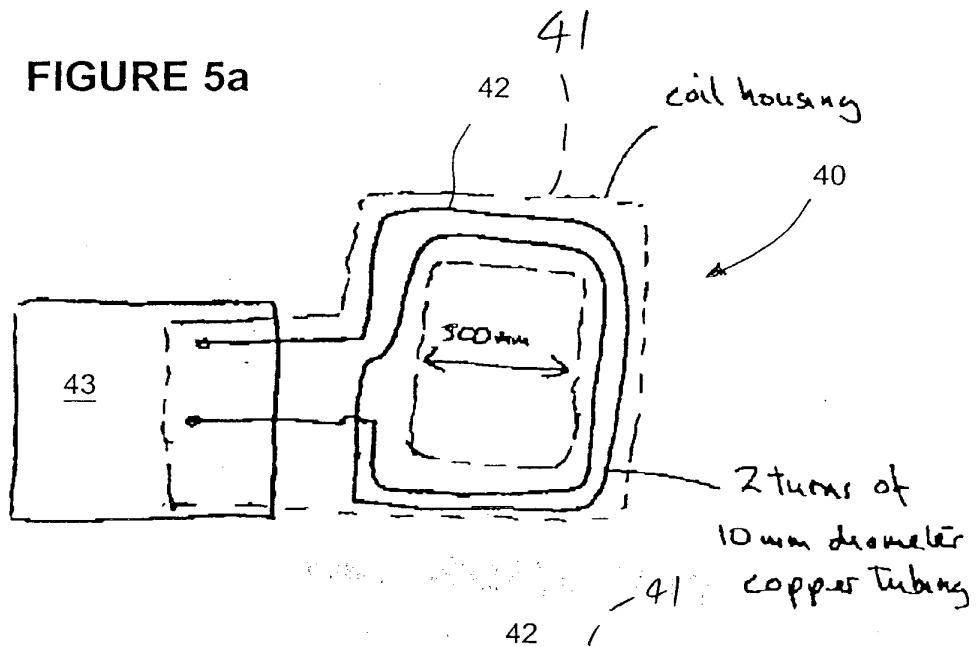


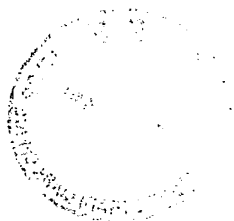
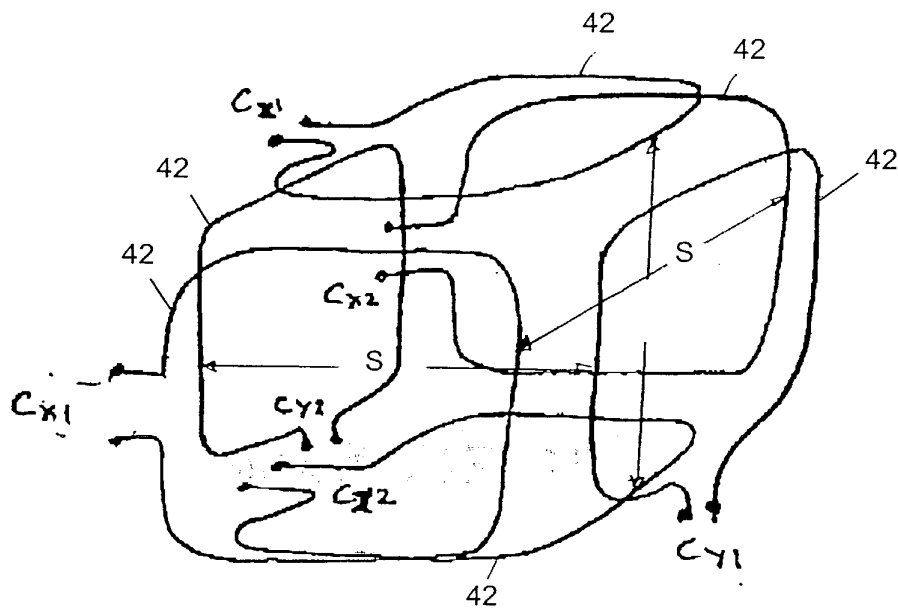
FIGURE 5b



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FIGURE 6



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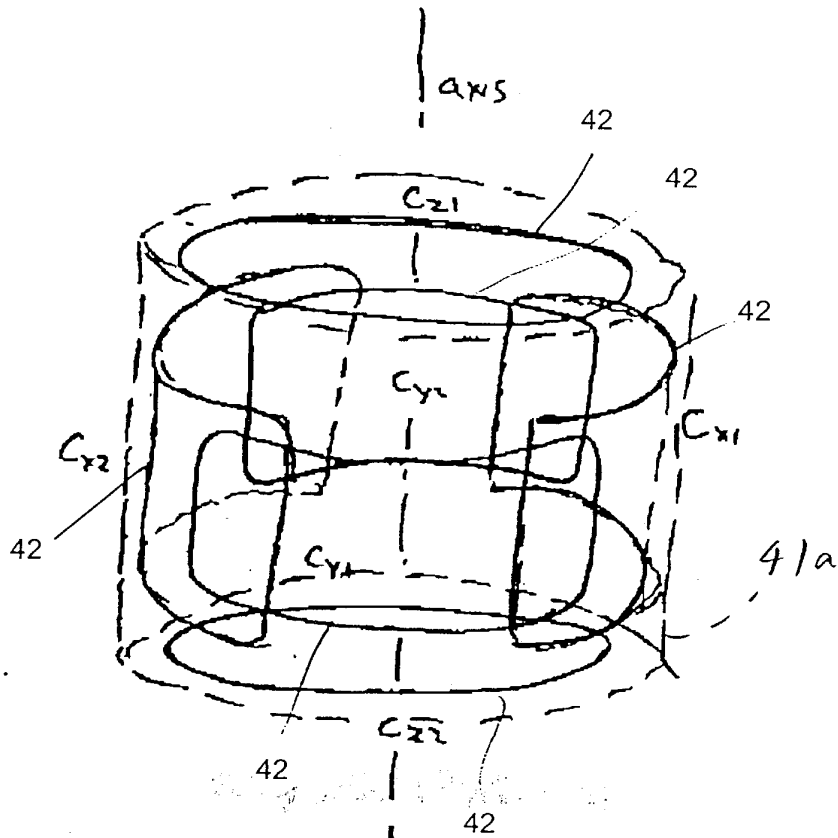


FIGURE 7

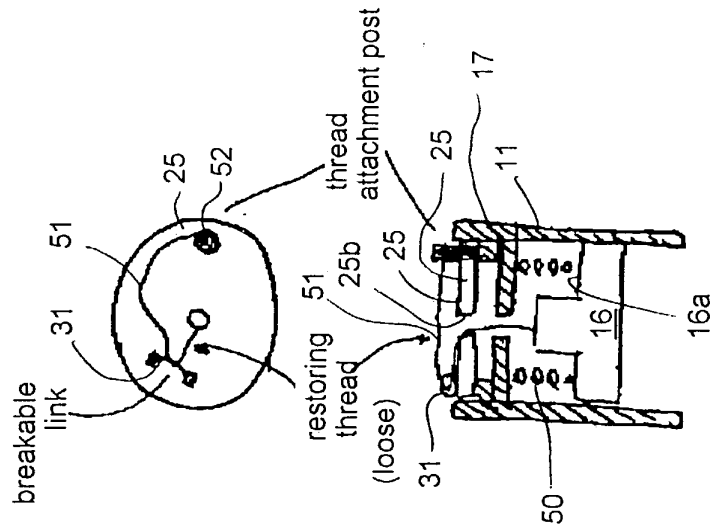


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FIGURE 8a



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FIGURE 8b

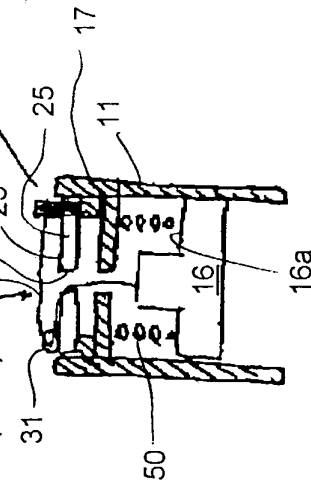


FIGURE 9a

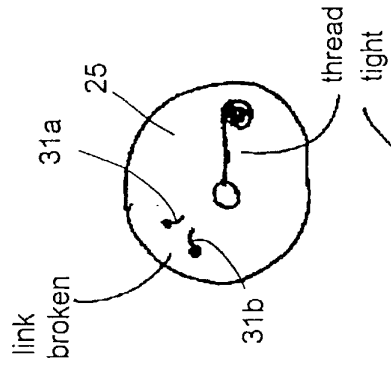
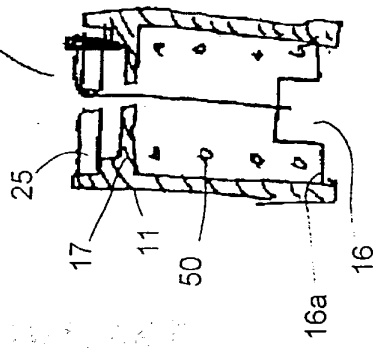


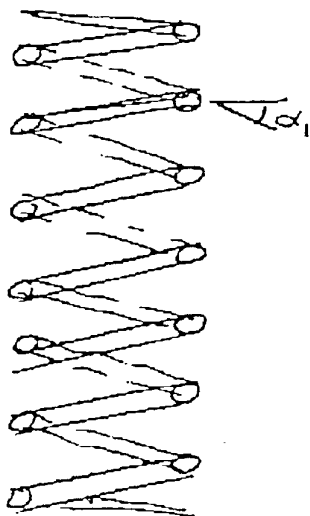
FIGURE 9b



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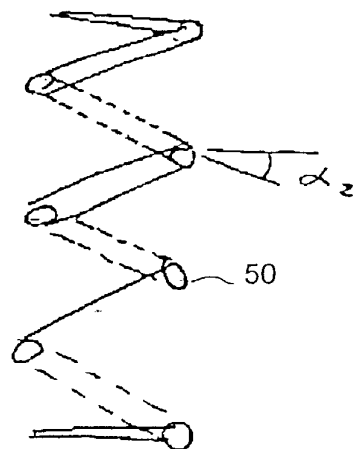




Conventional coil
spring

Figure 10a

Prior Art



Coil spring operating
at close to the yield point

Figure 10b

$$\alpha_2 > \alpha_1$$



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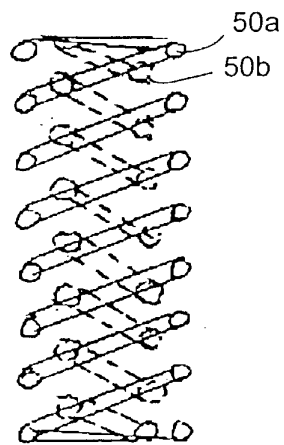


Figure 11a

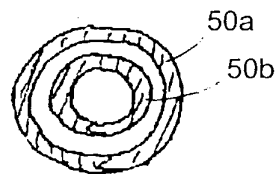
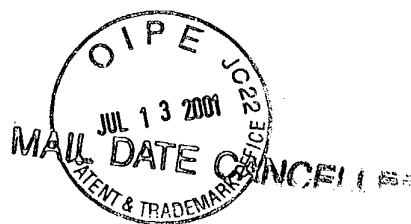


Figure 11b

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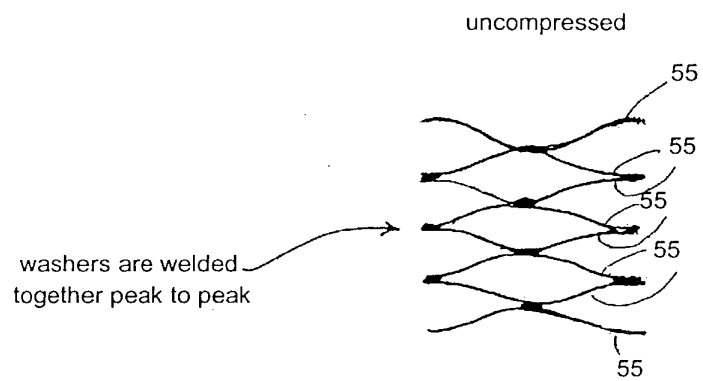


FIGURE 12a

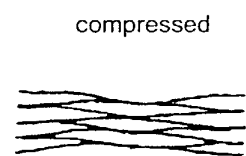


FIGURE 12b

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